Unveiling visionary frontiers: a survey of cutting-edge techniques in deep learning for retinal disease diagnosis

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ABSTRACT

Retinal disorders impact millions of people globally. These disorders can be detected and diagnosed early enough to not only cure but also avoid permanent blindness. Manual identification of these diseases has always been tedious, time-consuming, and inconsistent. For ophthalmologists, retinal fundus images are a valuable source of information in diagnosing retinal diseases. Automatic identification of eye disorders using artificial intelligence (AI) based learning models has seen substantial development in the computer vision sector recently. Various models, particularly deep learning (DL) models are incredible in identifying and classifying diseases. In the presented review, we have performed an in-depth analysis of various existing DL models, involving preprocessing, classification, segmentation, and techniques to deal with data imbalance. We have also endeavored to gauge the effectiveness of these models by evaluating their performance using the metrics employed in their assessment. In addition, we explored various challenges along with the potential future scope in this domain.

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1. INTRODUCTION

According to current estimates, there are approximately 2.2 billion individuals suffering from visual impairments across the globe. At least 1 billion of these cases could have been averted or whose causes have not yet been addressed, per the World Health Organization (WHO) [1]. The major causes of these diseases are attributed to ocular diseases. Vision loss and blindness have significant adverse social and psychological effects in all societies. Medical imaging is evolving rapidly and has a substantial impact on patient management today. The precise and timely diagnostics by this imaging technique have shown promising results in visualizing anomalies existing in the patient's body, determining disease stages, progression, and treatment planning. For instance, in ophthalmology, the availability of optical coherence tomography (OCT) is unparalleled. It has reduced the dependency on ophthalmologists' expertise and knowledge. Examining and grading the images manually is not just cumbersome and laborious; it could also lead to misinterpretation and the waste of health data. However, with the increasing volume and complexities of medical diagnostic imaging, interpretation and controlling retinal disease is more complicated due to the diverse images and findings that are recorded for individuals, and also the hypothesis that supports it [2].

While conventional diagnostic techniques were heavily based on the physician's ability to manually assess the medical data, modern clinical diagnostic techniques rely on intelligent technologies to manage the

medical data efficiently. Computer-aided diagnosis (CAD) and other artificial intelligence (AI) disciplines have proven to be highly productive in screening seemingly huge-scale data [2], [3]. Furthermore, AI has a substantial role in the field of ophthalmology, especially in diagnosis and therapy for retinal diseases because of its practical image interpretation [3], [4]. Retinal diseases vary widely based on categories and disease phases. Early detection is crucial for curable diseases, as overlooking them can lead to gradual vision loss and permanent blindness. Common retina diseases include diabetic retinopathy (DR), cataracts, glaucoma, age-related macular degeneration (AMD), retinal detachment, retinal tear, and macular hole. Limited clinical data availability makes refining the accuracy of medical imaging modalities challenging. However, with the advent of deep learning (DL), automated diagnosis of multiple retinal ailments has gained significant interest.

The study's remaining sections are structured as follows: Section 2 delves into the transition from traditional machine learning (ML) to DL, exploring various CNN models. Transfer learning, Multi-label classification, and Ensemble approaches are covered in Sections 3, 4, and 5, respectively. Section 6 addresses data imbalance through data augmentation techniques. Section 7 critically examines DL techniques, their performances, and vulnerabilities. The paper concludes in Section 8.

2. OUTLINE OF DL METHODS

A class of AI called ML trains the system to gain knowledge from the chunk of data, followed by accurate predictions without much human interference. It can further be classified as supervised, unsupervised, and reinforcement learning [5]-[9]. The conventional ML algorithms are shown in Table 1.

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|----------------|--|-----------------------------|---------------------------------|
| Classification | Description | Applications | Algorithms |
| Supervised | The system is trained with labeled | Classification, regression, | Linear Classifiers, SVM, Random |
| learning | datasets | and forecasting | Forest, Decision Tree, Logistic |
| | | | Regression, KNN, Naive Bayes |
| Unsupervised | The system is provided with datasets | Clustering and | k-means, PCA, Hierarchical |
| learning | that aren't precisely labeled | Dimensionality | clustering, Mean Shift |
| | | Reduction | |
| Reinforcement | Intelligent agent acquires behavior in | Modeling non-linear | ANN, Markov Decision Process, |
| learning | an uncertain, complex environment | relationships | Q-learning, |
| | through trial-and-error mechanism | in high dimensional data | Temporal difference learning |

Table 1. Classification of ML techniques

High-resolution images are crucial for disease identification and diagnosis applications. Conventional ML algorithms are inadequate due to the unpredictable traits of medical images. Their manual feature selection process and susceptibility to errors from overfitting/underfitting training datasets further hinder accurate predictions [8]. Among the techniques involving medical imaging, the one that has seen a breakthrough in recent years is DL. The major inspiration for DL, a subset of ML that resembles the structure of a human neuron, is the connectivity between neurons in the brain. The deep neural network comprises artificial neural nodes, organized into three layers: an input layer, multiple hidden layers, and an output layer, as illustrated in Figure 1. DL algorithms are capable of performing automatic feature extraction from large data sets to provide accurate results. Numerous DL techniques are available [10], [11] as depicted in the Table 2.



Figure 1. Architecture of deep neural network

| Table 2. Classification of DL techniques | | | | |
|--|--|--|--|--|
| Classification | Description | Applications | | |
| Deep belief networks | Machines are trained using labeled training data | Classification, regression, recognition, and forecasting | | |
| Convolution neural network | Machine analyses and cluster unidentified patterns without human intervention | Clustering and dimensionality reduction | | |
| Deep autoencoder | Machines are trained to analyze optimal behavior in their environment to make suitable decisions | Modeling non-linear relationships in high- dimensional data | | |
| Deep boltzmann Machine | Extension of RNN, additionally hidden layers and directionless connections between its nodes | Dimension reduction, categorization, regression, collaborative filtering, feature learning | | |
| Multi-layer Perceptron (MLP) | MLP has layers of activation-function equipped perceptions | Software for machine translation, image, and voice recognition | | |
| Radial basis Functions (RBFs) | RBFs are neural network activation used in RBFNs | Regression, categorization, timeseries forecast | | |

| Table 2. Classification of DL technique |
|---|
|---|

Assessing retinal illness severity relies on fundus datasets, but the raw image quality often lacks precision for minor changes. Noise removal, a critical initial step in fundus image processing, involves applying filters like mean, median, Gaussian, and Wiener to address image imperfections [12], [13]. Enhancing fundus images for precise detection of subtle variations in the retinal vasculature or advanced disease detection requires overcoming challenges like varying vessel lengths, branches, low contrast, and vessel crossings. In the Figure 2, the contrast enhancement comparison with respect to HE as shown in Figure 2(a), AHE as shown in Figure 2(b), and CLAHE as shown in Figure 2(c) is clearly depicted. CLAHE has gained popularity for effectively enhancing contrast in retinal vessels. It surpasses both AHE and conventional HE making it the preferred choice for performance improvement [14]-[19].



Figure 2. Comparison of contrast enhancement using HE, AHE, and CLAHE: (a) histogram equalization (HE), (b) adaptive histogram equalization (AHE), and (c) contrast limited adaptive histogram equalisation [20]

Various techniques employing CLAHE, involving top-hat and high-boost filters like Butterworth, Frangi, etc were used to eliminate Gaussian, salt-pepper noise and strengthen the red, green, and blue channels [20]–[23]. Techniques involving modified particle swarm optimization (MPSO), a fully attention-based network (FANet) were used on CLAHE to limit intra-class inconsistencies and improve segmentation results [24] A unique fundus image quality assessment and segmentation of OD using CNN and Grab cut algorithm was introduced. The model achieved an accuracy of 98.72%, 99.21%, and 96.43% on DRION, DRISHTI-GS, and RIM-ONE datasets respectively [25].

In the realm of DL, convolutional neural networks (CNNs) stand out significantly, particularly in applications related to computer vision. CNN architecture as shown in Figure 3, consists of input layers for image data, followed by convolutional layers that extract features. Pooling layers reduce spatial dimensions, and fully connected layers perform classification. ReLU activation functions introduce non-linearity, aiding in feature learning. CNNs excel in tasks like image recognition due to their hierarchical feature extraction [26]–[31]. Figure 3 depicts the standard framework of a Deep CNN model.

Liao *et al.* [32] proposed EAMNet, an interpretable model for efficient glaucoma diagnosis. EAMNet includes a CNN backbone for feature extraction, multi-layer average pooling (M-LAP) for connecting semantic and location information, and evidence activation mapping for detection and identification. It achieved an accuracy of 0.88, surpassing contemporary diagnostic techniques. Kou *et al.* [33] suggested an enhanced residual U-Net (ERUNet), for the segmentation of Microaneurysms (MA) and Exudates (EX). ERU-Net generates three U-paths, each made up of three up-sampling paths and one down-sampling path. ERU-Net improves the associated feature fusion and captures the nuances of fundus images with its three U-path structures. Bilal *et al.* [34] introduced a mixed model for DR grading. Three classifiers were used in the classification phase: A model combining support vector machine (SVM), k-nearest neighbor (KNN), and binary tree (BT) models, along with a majority voting method to acquire the final output. Multiple diagnoses from disease grading databases were employed to complete this project, which led to an accuracy of 98.06%, sensitivity of 83.67%, and specificity of 100%. Islam *et al.* [35] developed a multi-stage CNN-based system called DiaNet based on a pre-trained CNN model on ImageNet to diagnose diabetes mellitus.



Figure 3. Architecture of a typical deep convolutional neural network

Additional layers were inserted to improve its ability to recognize more complicated patterns in the input. The model is primarily finetuned for DR identification. DiaNet uses Dense-Net as its base CNN and performs multistage fine-tuning to provide a high degree of accuracy of 84.4%. Xu *et al.* [36] introduced a global-local attention network (GLA-net) to tackle the classification of cataracts. The system proposes two subnet levels, global-level attention emphasizes global structure information, and local attention network focuses on discriminative features of specific regions. The model achieved a detection accuracy of 90.65%, grading accuracy of 83.47% and classification accuracy of 81.11%. Zamani *et al.* [37] observed the lack of extensive analysis in the field of pterygium identification using DL and proposed a new framework, VggNet16-wbn, a CNN-based trained network obtained from VggNet16. A network analysis of six pre-trained CNN networks to recognize pterygium led to the presentation of a new CNN-based network architecture. Moosawi and Khudeyer [38] proposed ResNet-n\DR by modifying and adding three residual units to Resnet-34. The proposed model achieved 93.5% accuracy, 90.7% sensitivity, 98.2% specificity, 90.1% F1 score, and 89.5% precision on APTOS-2019 dataset. For maximum performance, DL approaches require large-scale databases to be implemented. Because of data-acquisition elements and other needs, acquiring large-scale images or datasets in various domains, particularly in medical imaging, is a challenging and time-consuming operation.

3. TRANSFER LEARNING

Transfer learning (TL) is a standard technique that is comparable to DL in computer vision as well as natural language processing (NLP) jobs [39]. The foundation of the image classification problem comprehends the training, validation, and testing phases of DL algorithms. The DNN training procedure can be carried out with either new or existing CNN-trained networks as training datasets. Learning from scratch requires a manual network to be built and the structure of DNN to be clearly understood [40]–[42]. Additionally, a large volume of data sets is required. TL is an alternative to training data from the outset, which necessitates large-scale data, for compact data representations in DL [43]. Jabbar *et al.* [44] introduced a VGG-16-based TL model to enhance the classification performance of DR. The model was trained using EyePACS and Kaggle datasets. The model achieved an accuracy of 96.61% which was way higher than the accuracies of ResNet, AlexNet, and GoogleNet. Alghamdi and Mottalebet [45] proposed an automatic glaucoma diagnosis framework using three CNN models— Transfer CNN (TCNN), semi-supervised CNN with self-learning (SSCNN), and semi-supervised CNN with autoencoder (SSCNN-DAE). TCNN transfers knowledge from VGG-16 to a small dataset, SSCNN uses self-learning, and SSCNN-DAE employs a denoising autoencoder for feature extraction. Results show SSCNN-DAE outperformed TCNN and SSCNN, achieving accuracy rates of 93.8%, 91.5%, and 92.4%, respectively.

4. MULTI-LABEL CLASSIFICATION

Multi-label classification (MLC) is regarded as a prominent topic in the research field, especially in the world of computer vision, particularly medical imaging analysis. In MLC, an object can be classified into more than one class. There is no restriction on the number of labels a subject could be assigned in the multi-label problem. We use a range of multi-label classification-specific methodologies to overcome these challenges:

- a) Problem transformation: It is the way of transforming a multi-label dataset into a single-label dataset. Machine-readable single-label datasets make it easier to create models. The following techniques are used to transform problems:
- Binary relevance: This technique considers every label independently, and MLC is used to separate them.
- Classifier chain: It is a sequential process in which one classifier output is used as the input for the next classifier in the chain.
- Label power set: It changes the problem to a multi-class problem. The unique label combinations found in the data are then used to train each multi-class classifier.
- b) Adapted algorithms: This technique uses the algorithm adaption method to perform MLC.
- c) Ensemble model: This is a hybrid method that combines the capabilities of both the above techniques.

Abdelmaksoud *et al.* [46] proposed a multi-label CAD system for detecting and diagnosing DR. The system standardizes retinal image sizes, utilizes GLRLM to extract texture features from pre-processed fundus images, and employs U-Net for automatic detection of exudates, MA, haemorrhages, and blood vessels. Six features are extracted, and a classifier chain ML-SVM is employed to distinguish between different DR grades. Fu *et al.* [47] presented M-Net, a one-stage multilabel system for optic disk (OD) and optic cup (OC) segmentation. M-Net incorporates a U-shaped CNN, multi-scale input layer, side-output layer, and a multilabel loss function. The input layer generates a pyramid representation for various receptive field sizes, and a U-Net model trains the hierarchy structure. The side-output layer acts as an initial classifier, providing local forecast maps for different scale layers. A multi-label loss function yields the final segmentation map, and polar transformation enhances segmentation performance by providing an image depiction in polar coordinates. The system demonstrated satisfactory performance in glaucoma screening on ORIGA and SCES datasets during testing.

Lin *et al.* [48] proposed two MLC schemes: MCG-Net, using graph convolutional networks, and MCGS-Net, combining graph convolutional networks with self-supervised learning. MCG-Net-GCN captures crucial information from multi-label fundus images, while MCGS-Net enhances classification with self-supervised learning. Tested on ODIR and SSL datasets, both demonstrated superior categorization, achieving a 4.74% boost in recall. MCGS-Net exhibits stronger generalization, especially for unseen fundus picture collections. Wang *et al.* [49] introduced Efficient-Net for precise identification of fundus abnormalities in retinal images. It comprises a feature extraction network that scales depths, widths, and resolutions efficiently. The second component is an ML classification neural network with a unique structure. The final classification result is obtained by blending outcome probabilities from various models. Training and testing were conducted using the ODIR 2019 dataset, showing superior outcomes even when trained on fewer datasets [49]. Using MLC and a graph convolutional network (GCN), this model identified eight fundus lesion types in color images.

It consists of a CNN-based Res-Net-101 for image feature extraction and a GCN for classification, utilizing matrices from label embeddings and co-occurrence patterns. The model accurately recognized various lesions, including hemorrhages, laser scars, retinal arteriosclerosis, micro-aneurysms, and hard/soft exudates [50]. MLC-driven gradient-weighted class activation mapping (Grad-CAM) was developed by Jiang *et al.* [51] and it could classify and automatically detect the DR regions with different lesions. First, DR lesions were used as labels for the collection of additional learning data. Second, lesion identification was accomplished by combining Grad-CAM and multi-label classification. They formed a Res-Net-based DL model and achieved 94.4% specificity and 93.9% sensitivity.

5. ENSEMBLE LEARNING

The fundamental idea behind ensemble methods is a linear combination of numerous model-fitting approaches as opposed to only using single-fit. Ensemble learning includes various learning models to achieve better predictive performance than a single model. Ensemble methodologies are broadly classified as Homogeneous Ensemble approaches, involving Bagging and Boosting, Heterogenous Ensemble approaches involving Stacking, and Majority voting algorithms [52]–[55].

- BAGGing: This technique creates an ensemble model through aggregation and bootstrapping, adapting similar learners to small sample populations and using majority voting to combine predictions.
- Boosting: An iterative method aimed at reducing bias error, boosting builds a robust predictive model by adjusting the weights of previous classifications, though it may lead to overfitting.
- Stacking: This method optimally combines predictions from diverse high-performing ML models.
- Majority voting algorithm: Enhancing efficiency through voting, this method determines the final prediction based on the majority vote from each learning algorithm [52], [54].

To enhance the model's prediction, Qummar *et al.* [56] suggested a combination of five DCNN models (Resnet50, Inception-v3, Xception, Dense121, and Dense169) are trained to classify different DR stages by encoding the rich information. Lyu *et al.* [57] proposed a training method for categorizing multiple labels with varying sample sizes and difficulty levels. They calculate inverse frequencies for each category to guide model training. The model is iteratively trained with adjusted class weights, addressing flaws and emphasizing challenging samples. Experimental results from RIADD-2021 yielded an 88.24% accuracy [57].

6. DATA AUGMENTATION TECHNIQUES

The scarcity of substantial, freely available retinal image datasets has been a stumbling block to successful AI implementation. The majority of publicly accessible datasets contain fewer than a thousand images. Since the most crucial necessity of automated retinal disease diagnosis is its affordability and extensive screening of the general public, these automated solutions should be capable of performing well in actuality with fundus images captured in everyday practice with little constraints [58]. Despite several publicly available datasets, there remains a scarcity of large, diverse, and accurately annotated datasets, particularly for severe cases like PDR and Macular Edema. One potential solution to this problem is synthesizing data through augmentation techniques, involving fundamental image manipulations such as translation, scaling, rotation, and elastic deformation applied to original training data samples [59].

Generative adversarial networks (GANs) have made breakthroughs in retinal image synthesis in recent years. GANs are built with two models in mind: a generator and a discriminator [60]. The generative model creates realistic images from random noise, while the discriminative model distinguishes between authentic and generated images. The generator tries to deceive the discriminator by producing realistic visuals, and the discriminator strengthens its ability to avoid being misled [61], [62].

A 2-stage GAN for high-resolution retinal images was introduced by Andreini *et al.* [63]. The suggested model employs a two-step procedure: Primarily, a GAN is trained to provide semantic label maps that describe the vasculature as it grows over time. Second, realistic retinal images are produced from generated vasculature using an image-to-image translation method. In DR patients, the majority of cases are mild or moderate NPDR, with only 5% corresponding to PDR. Due to the scarcity of PDR lesions for model training, Araujo *et al.* [59] introduced a heuristic-based data augmentation approach. They utilized a neo-vessel generation algorithm to synthesize neo-vessel (NV)-like structures. The DRGraduate model for DR grading was trained with this data augmentation technique, and experiments were performed to assess its impact [64]. Chen *et al.* [65] introduced RF-GANs, comprising two generative models, RF-GAN1 and RF-GAN2. RF-GAN1 addresses the domain gap between semantic segmentation datasets and EyePACS. It utilizes HR-Net to enhance high-resolution representation through continuous multi-scale fusion across parallel convolutions, preserving high-resolution features by integrating parallel convolutions from high to low resolution.

7. LIMITATIONS OF EXISTING TECHNIQUES AND FUTURE DIRECTIONS

According to the review conducted in this study, we determine the following areas for further research investigations:

- a) Lightweight neural network architectures: While many DL methods for retinal ailments exhibit exceptional performance, their efficiency is often accompanied by high computational resource consumption. Addressing this challenge is crucial to reduce computing requirements without compromising the model's performance.
- b) Image synthesis using data augmentation approaches: Another concern arises from the use of small datasets in the evaluation of many techniques. The performance of models on large databases remains uncertain when implemented, compounded by issues of dataset imbalance and limited sample availability. Traditional data augmentation and class balancing techniques are insufficient to address this challenge, highlighting the need for more effective augmentation methods to enhance diagnostic performance.
- c) Strengthening generalisability: Most of the systems have to deal with the overhead of pre-processing and post-processing stages. So, effective models need to be developed to standardize techniques in terms of implementation, performance, and accuracy and also to accept retinal images of varying sizes in datasets.
- d) Disease-based system rather than lesion-based system: The majority of the existing work we see today is mainly based on DR detection and classification of lesion types. Likewise, there is considerable work on glaucoma detection as well. Works relevant to diseases like retinitis pigmentosa, retinoblastoma, macular hole, retinal tear, retinal detachment, and some other rare syndromes and genetic eye disorders are not explored. So, there is a need to devise disease-based models rather than lesion-based models [46].
- e) Integrating deep CNN and active learning framework: To drastically reduce annotation effort, a deep active learning system that integrates fully the CNN model and active learning may be created. Active learning would assist in deciding which images need annotation to acquire outstanding performance with a low budget and quantity of time [66].

Ocular disease diagnosis is evaluated and validated using various performance metrics like Accuracy, Sensitivity, Specificity, F1-Score, and Dice Similarity. Figure 4, depicts the performance evaluation of the various DL techniques. Table 3 (in Appendix) we have summarized various DL approaches, datasets, their performance and shortcomings presented in this study.



Figure 4. Performance evaluation of DL techniques discussed in this study

8. CONCLUSION

Medical imaging has evolved into a primary tool for clinical and differential diagnosis, with significant advancements. This paper provides a comprehensive summary of diverse DL techniques for ocular disease diagnosis, classification, and segmentation, ranging from traditional ML to advanced methods like CNN, Transfer Learning, Ensemble Learning, and MLC. The discussion includes strategies to address data scarcity, such as augmentation techniques and the use of GANs for generating comparable images. The analysis highlights significant methodological variations in pre-processing, classification, segmentation, and performance evaluation. Notably, most DL methods discussed apply to specific pathological conditions, posing a challenge for universal disease detection in the clinical context.

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APPENDIX

Table 3. Summary of various DL techniques, performance, and shortcomings (continue)

| Reference | Aim | Technique | Dataset | Performance | Shortcoming |
|-----------|------------------|-------------------------|---------------|---|----------------------------|
| [15] | Contrast | Triangular Fuzzy | CASIA-IRIS | Mean Squared Error - | The clipping value varies |
| | Enhancement | Membership-CLAHE | | 0.0006 | according to the image, |
| | | | | Peak-Signal-to-Noise- | the limiting factor is |
| | | | | Ratio -42.2291 | image-dependent |
| [24] | Contrast | CLAHE-MPSO | DRIVE, | Sensitivity-83.15% | A fixed Scale value of |
| | Enhancement | | STARE | Specificity-84.33% | optimization |
| [(7]) | C , , , | | OT A DE | Accuracy-97.50% | |
| [67] | Contrast | Upgraded CLAHE, | STARE | Sensitivity-100% | Unly applicable for 5 |
| | Ennancement | ICININ RESINCTION | | Accuracy 100% | lesion conditions |
| [68] | Contrast | Fuzzy Clipped | MIAS | Peak-signal-to-noise ratio | The complex chosen clip |
| [00] | Enhancement | CLAHE | 1011116 | (PSNR)-18.735 | point isn't block adaptive |
| | | | | Discrete Entropy-5.633 | F |
| [35] | Distinguish | Multi-Stage CNN | EyePACS, | Accuracy-84% | Cannot distinguish |
| | healthy and | called Dia-Net | QBB | Sensitivity-85.86% | lesions and stages of DR |
| | diabetic eye | | | Specificity-83.06% | |
| | | | | F1-Score-84.71% | |
| [33] | MA and Exudates | Enhanced residual U- | E-Ophtha, | Area under the curve | Applicable only to MA |
| | (EX) | three up campling and | IDRID, and | (AUC) of 0.9956, 0.9962, 0.0801 for MA and | and EX, other lesion |
| | segmentation | three down-sampling | DDK | 0.9801, 101 WA and | could be misclassified |
| | | naths | | Ex | could be inisclassified |
| [34] | DR detection and | Mixed models (SVM, | IDRiD | Accuracy-98.06% | Strong reliance on feature |
| | Classification | BT and KNN) is | | Specificity-100% | extraction and pre- |
| | | applied for | | Sensitivity-83.67% | processing processes. |
| | | classification | | | |
| [69] | DR Grading | CAB for | DDR, | Accuracy- | Challenging to find tiny |
| | | discriminative regions | Messidor, | 0.7813, Kappa- | lesion spots owing to the |
| | | and GAB for global | EyePACS | 0.7699 | image supervision level. |
| | | attention features | | | Can only provide grading |
| [37] | Ptervoium | VaaNet16-whn model | OPKOM-26 | $\Delta ccuracy - 99.2\%$ | Limited dataset with |
| [37] | Detection | with additional batch | UBIRIS | Sensitivity-98.45% | questionable clinical |
| | Dettection | normalization layers on | ODING | Specificity-100% | applicability |
| | | TL | | I S S | |
| [36] | Cataract | GLA-net based on | 9912 retinal | Detection accuracy - | Extensive supervision is |
| | Detection | two-level subnets | fundus images | 90.65% | required for detection and |
| | | focussing on Global | from Beijing | Grading Accuracy-83.47% | grading tasks involving |
| | | level attention and | Tongren Eye | Classification Accuracy- | global and local attention |
| | | local-level attention | Center | 81.11% | models, and limited data |
| | | models | | | the problem |
| [32] | Glaucoma | EAM-net based on | ORIGA | Accuracy-0.88 | High-resolution maps are |
| [52] | Diagnosis | multi-laver average | ondon | OD segmentation (Dice)- | hard to represent. |
| | 8 | pooling (M-LAP) | | 0.9 | Besides, Optic cup |
| | | 1 0 0 0 | | | segmentation is |
| | | | | | completely ignored |
| [70] | Glaucoma | Fuzzy Broad Learning | RIM-ONE-r3, | DC Score of 0.953,0.856 | Cannot eliminate noisy |
| | detection (Optic | | SCRID | for OD and OC, | images, to accomplish |
| | cup (OC) and OD | | | and AUC of 0.906 and | segmentation, individual |
| | segmentation) | | | 0.923 | channels must be |
| [71] | Glaucoma | Compactly self- | ACRIMA | E1 score of 100% 73.9% | Must be tuned and pre- |
| [/1] | Diagnosis | organized Operational | RIM-ONE | 93.9% | trained for the |
| | Diagnoois | Neural Networks (Self | ESOGU | for ESOGU. RIMONE | classification issue. |
| | | -ONNs) | | and ACRIMA | |
| [72] | Glaucoma | CDeD-Net cup-disc | DRISHTI-GS, | Sensitivity-95.67%, 99.81% | A large number of |
| | Screening | encoder for combined | RIM-ONE | for OC, 97.54%, 99.73% for | unlabelled targets are |
| | | OC | | OD on Drishti, 95.17% and | needed. The model's |
| | | and OD segmentation | | 99.81% for OC, | applicability to diverse |
| | | | | 97.34%,99.73% for OD on | datasets is questionable. |
| [73] | Glaucoma | Five distinct | ACRIMA | AUC of 0.9605 ofter | Performance worsened |
| [13] | Screening | ImageNet | ACININA | ontimizing Xcention | when tested on different |
| | Sereening | trained CNNs as | | architecture, with a | datasets. |
| | | glaucoma classifiers: | | 95.92~97% confidence | |
| | | VGG16,19, ResNet50, | | | |
| | | InceptionV3, | | | |
| | | Xception. | | | |

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| Reference | Aim | Technique | Dataset | Performance | Shortcoming |
|-----------|-----------------------|---------------------------|-------------------------|--------------------------|--------------------------------|
| [74] | Multi-class | (ANU-net-FPOA) | University of | Accuracy-98.7% | Though the proposed |
| | AMD | Atten -tion based U- | California San Diago | Specificity-99.8% | model successfully |
| | (Drusen | net, (FPOA) Flower | San Diego | Sensitivity-99.7% | CNV it was upable to |
| | (Drusen, Choroidal | optimization algorithm | (UCSD) | | classify cases of Macular |
| | Neovasculariz | for hyperparameter | | | Edema (DME) |
| | ation (CNV)) | tuning Squeeze-net | | | Edolika (DiviE) |
| | | for classification task | | | |
| [75] | Retinal | Multi-modal | DRIVE, | Accuracy -97.40% on | Performs segmentation |
| | Vessel | framework | STARE, | Drive, 98.27%, 97.78%, | based on 2D connectivity |
| | Segmentation | ELEMENT with | CHASE-DB, | 98.34%, 98.04% and | features, not applicable for |
| | | connectivity and | IOSTAR, | 98.35% on STARE, | 3D Vessel segmentation. |
| | | region-growing | VAMPIRE FA, | CHASE-DB, | |
| | | features | RC -SLO | VAMPIRE FA, | |
| [46] | Pathological | MI CAD system using | ם:ח | A course of 1% | Applicable only for DP |
| [40] | changes and | U-Net based | DIARETDR1 | AUC-91.9% | and its classification |
| | diagnosing | Multilabel SVM and | DIARLIDDI | sensitivity-86.1% | doesn't work well for other |
| | DR stages | classifier chain | | specificity-86.8%. | retinal disease |
| | 0 | | | dice score-86.2% | |
| [49] | To identify | Efficient Net model | ODIR 2019 | Accuracy-0.90, | Works well with limited |
| | one or more | with CNN based | | AUC-0.67, | number of datasets, clinical |
| | retinal | multilabel | | F1Score- 0.85, | applicability is still an open |
| | disorders | classification | | Kappa-0.43 | issue. |
| [50] | Diagnosis of | Graph neural network | 7459 fundus | F1 Score -0.808, | Model demonstrated a |
| | multiple | - based ML | images from | AUC- 0.986, 0.954, | lackluster performance for |
| | Tundus lesion | classification to | 2282 patients | 0.946, 0.957, 0.952, | MA, soft, and hard EX |
| | | types of retinal lesions | create a corpus | 0.889, 0.957, and | detection |
| | | types of feutial festolis | of fundus data | 0.920 | |
| [51] | DR lesion | ML classification | 3228 fundus | Sensitivity-93.9%. | Ineffective for bright and |
| [] | classification | including a mechanism | images were | Specificity-94.4% | low-light fundus images |
| | and detect | for gradient-weighted | collected | 1 2 | don't work for PDR cases |
| | lesion region | class activation (Grad- | | | |
| | | CAM) using ResNet | | | |
| [57] | Identifying | A heuristic stacking | RFMiD | Accuracy-88.24% | Works well for the RFMiD |
| | multiple and | technique based on | | | dataset, but it is uncertain |
| | coexisting | multi-label ensemble | | | how well it performs with |
| | disassas | learning | | | different datasets. |
| [59] | Synthesis of | Heuristic-based Data | Messidor-2 | kappa value-0.78.0.74 | Misclassifies PDR signs |
| [07] | PDR cases in | Augmentation scheme | Kaggle | 0.70 in SCREEN-DR. | with (retinal hemorrhages |
| | DR | | SCREEN-DR | Kaggle, Messidor-2 | and fibrosis). |
| [63] | High- | Two Stage GANS | DRIVE, | AUC-98.65%,99.16% | Performance comparison is |
| | resolution | with progressively | CHASE_DB | Accuracy-96.90%, | not convincing due to the |
| | retinal image | growing GAN and | | 97.72% in DRIVE, | varied experimental setups |
| | generation | image translation | | CHASE | |
| [65] | Synthesis of | Two generative | EyePACS | Increase in | Doesn't work well with |
| | DR images | adversarial models | | Accuracy-1.53% | low-illumination images |
| | | DE GAN2 | | карра-1.70% | of vessel trees affects |
| | | RI-OAN2 | | | image synthesis |
| [76] | Automatic | Two-level hierarchical | 249.620 fundus | F1 score- 0.923 | Weak image segmentation |
| [, 0] | detection of | system constituting | images from | Sensitivity -0.978, | and locality of lesions were |
| | 39 retinal | CNNs and Mask- | various hospitals | Specificity - 0.996 | not accurately identified |
| | conditions | RCNN | in China, the US, | Accuracy-87.98 | 2 |
| | | | and databases like | | |
| | | | Messidor, IDRiD, | | |
| | a | | and Refuge. | | - |
| [77] | Segmenting | SL-EACM: Saliency- | CHASE-DB | Accuracy of 0.994, | The suggested approach |
| | OD IOr Glaucoma | Level set with | DRIUN-DB | 0.992, 0.991, and Dice | smaller ODs. Palaseting |
| | Diagnosis | modified Active | 0713011-031 | 0.970 on Chase Drion | the priors would avert this |
| | Diagnosis | Contour Model | | and Drishti respectively | issue |
| [78] | Detection of | Exudates detection | DIARETDB0 | Accuracy-98.2% | The model's evaluation |
| [, 0] | DR lesion | using binary operation | DIARETDB1 | Specificity-96.96% | focused on 75 selected |
| | (Hard | and fuzzy-based | | Sensitivity-98.10% | DiaretDB0 images for |
| | exudates) | classification | | - | exudate classification, |
| | | | | | prompts questions about its |
| | | | | | performance in the |
| | | | | | presence of other lesions |

d shortcomings (c f. Table 3 S DI toohnig formance ontinuo)

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